Multiple-Quantum Line Narrowing for Measurement of $H^{\alpha}-H^{\beta}$ J Couplings in Isotopically Enriched Proteins

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Abstract: Uniform ¹³C enrichment of proteins is commonly used for NMR studies of proteins that are not amenable to conventional homonuclear 2D NMR spectroscopy. In such studies, the one-bond ¹H-¹³C dipolar interaction is usually the dominant source of ¹H line broadening. ¹H-¹³C zero- and double-quantum coherences are, to first order, not affected by this dipolar relaxation mechanism. The relatively long relaxation time of such ¹H^{α}-¹³C^{α} multiple-quantum coherences is exploited for measurement of H^{α}-H^{β} J couplings in a sample of uniformly ¹³Cenriched calcium-free calmodulin (16.7 kD) and a sample of TGF- β 1 (25 kDa). $J(H^{\alpha}-H^{\beta})$ provides information on the stereospecific resonance assignment for residues with nonequivalent H^{β} methylene protons and on the χ_1 torsion angles.

Uniform ¹³C enrichment of proteins makes it possible to record highly sensitive 3D and 4D analogs of conventional 2D COSY, TOCSY, and NOESY NMR spectra.^{1,2} Spectral dispersion in the added ¹³C dimension(s) greatly alleviates the resonance overlap problem of conventional 2D NMR and makes it possible to study the structure of proteins in the 10-30 kDa range. However, enrichment with ¹³C has a deleterious effect on the ¹H line width, resulting from the large one-bond ¹H-¹³C dipolar coupling which, in diamagnetic proteins, represents the dominant source of transverse ¹H relaxation. In the slow tumbling limit, relaxation of ¹H-¹³C zero- and double-quantum coherence is, to first order, not influenced by the dipolar coupling between the two nuclei.³ In macromolecules the relaxation time of one-bond ¹H-13C zero- and double-quantum coherence therefore is expected to be longer than for the singlequantum coherence of the individual ¹H and ¹³C spins. An analogous increase in the relaxation time of ¹H-¹⁵N multiplequantum coherence over the amide proton T_2 was exploited to obtain a modest increase in H^N-H^a COSY cross peak intensities of ¹⁵N-enriched proteins,⁴ and for minimizing signal loss in ${}^{3}J(H^{N}-H^{\alpha})$ -modulated ${}^{1}H-{}^{15}N$ shift correlation experiments, aimed at measurement of ${}^{3}J(H^{N}-H^{\alpha})$.^{5,6} For ${}^{1}H-\{{}^{13}C\}$, the heteronuclear dipolar broadening is about four times larger and therefore the difference between multiple-quantum and singlequantum relaxation is also much larger.^{7,8} Here we demonstrate

- (3) Griffey, R. H.; Redfield, A. G. Q. Rev. Biophys. 1987, 19, 51-82.
 (4) Bax, A.; Kay, L. E.; Sparks, S. W.; Torchia, D. A. J. Am. Chem. Soc. 1989, 111, 408-409.
- (5) Billeter, M.; Neri, D.; Otting, G.; Qian, Y. Q.; Wüthrich, K. J. Biomol. NMR 1992, 2, 257-274.
- (6) Kuboniwa, H.; Grzesiek, S.; Delaglio, F.; Bax, A. J. Biomol. NMR **1994**, 4, 871-878.

(8) Seip, S.; Balbach, J.; Kessler, H. J. Magn. Reson. 1992, 100, 406-410.

that use of ${}^{1}H^{-13}C$ multiple-quantum coherence indeed results in a large enhancement of resonance intensities in a quantitative $H^{\alpha}-H^{\beta}$ J correlation spectrum. Such a spectrum yields quantitative values for three-bond $H^{\alpha}-H^{\beta}$ J couplings, $J_{\alpha\beta}$, which are important for stereospecific assignment of nonequivalent C^{β} methylene protons and provide information on the side chain χ_{1} torsion angles.

Description of the Pulse Scheme

The pulse scheme for the 3D ¹³C^{α}-separated H^{α}-H^{β} in-phase COSY (HACAHB-COSY) pulse sequence is shown in Figure 1. Analogous to the HNHA experiment,⁹ proposed for measurement of ³J(H^N-H^{α}), the HACAHB-COSY scheme produces in-phase cross peaks and diagonal peaks, and the ratio of their integrated intensities provides a direct measure for $J_{\alpha\beta}$.^{10,11} The operator formalism description of this experiment is analogous to that of the HNHA experiment, and a detailed description is therefore not repeated.

The HACAHB-COSY scheme is of the so-called "out-andback" type,¹² where magnetization originates on H^α and is also detected as H^α magnetization during data acquisition. Briefly, the experiment functions as follows: The first $90_{\phi_1}({}^1\text{H})-\Delta 90_x({}^{13}\text{C})$ pulse pair converts H^α magnetization into a heteronuclear H^α_xC^α_y spin operator product wich represents the sum of H^α-C^α zero- and double-quantum coherence. Temporarily ignoring the effect of ${}^{13}\text{C}^{\alpha}$ chemical shift evolution, this coherence dephases between time points *a* and *c* due to homonuclear H^α-H^β J coupling, resulting in an operator product of the form H^α_xC^α_y. The relative amplitude of these two coherences is tan($2\pi J_{\alpha\beta}\delta$). The subsequent $90_{\phi_1}-t_2-90_{\phi_4}$ sequence, applied

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⁽¹⁾ Clore, G. M.; Gronenborn, A. M. Prog. NMR. Spectrosc. 1991, 23, 43-92.

⁽²⁾ Edison, A. S.; Abildgaard, F.; Westler, W. M.; Mooberry, E. S.; Markley, J. L. Meth. Enzymol. 1993, 239, 3-79.

⁽⁷⁾ Bax, A.; Ikura, M.; Kay, L. E.; Torchia, D. A.; Tschudin, R. J. Magn. Reson. 1990, 86, 304-318.

⁽⁹⁾ Vuister, G. W.; Bax, A. J. Am. Chem. Soc. **1993**, 115, 7772-7777. (10) Bax, A.; Max, D.; Zax, D. J. Am. Chem. Soc. **1992**, 114, 6924-6925.

⁽¹¹⁾ Bax, A.; Vuister, G. W.; Grzesiek, S.; Delaglio, F.; Wang, A. C.; Tschudin, R.; Zhu, G. *Meth. Enzymol.* **1993**, *239*, 79-105.

⁽¹²⁾ Ikura, M.; Kay, L. E.; Bax, A. Biochemistry 1990, 29, 4659-4667.

Figure 1. Pulse scheme for the 3D HACAHB-COSY experiment. Narrow and wide pulses denote 90° and 180° flip angles, respectively. Unless indicated otherwise, all pulses are applied along the x-axis. The phase cycle is as follows: $\phi_1 = 2(x), 2(-x); \phi_2 = x; \phi_3 = x, y, -x, -y;$ $\phi_4 = 4(x), 4(-x)$; receiver = x,2(-x),x. Quadrature detection in t_1 and t_2 is obtained by incrementing ϕ_2 and ϕ_1 , using States-TPPI. ¹³CO decoupling is preferably carried out with a selective composite pulse decoupling scheme,^{20,25} but due to hardware problems a 2 kHz CW field was used instead. Note that ¹³CO decoupling during t_1 induces a significant Bloch-Siegert shift (~0.7 ppm) in F_1 . Delay durations: κ = 1.5 ms; $T^{1} = 5.25$ ms; $T^{11} = 8.75$ ms; $\delta = T^{11} + 2\tau_{90}^{C}$; $\delta' = T^{11} - 2\tau_{90}^{C}$ $2\tau_{90}^{\rm H}$; $\Delta = \delta + 2\tau_{90}^{\rm H} - T^{\rm I} - \tau_{90}^{\rm C}$; $\Delta' = \delta' - T^{\rm I} - 3\tau_{90}^{\rm C}$, where $\tau_{90}^{\rm C}$ and τ_{90}^{H} , are the 90° ¹³C and ¹H pulse durations. Pulsed field gradients (PFG) are all sine-bell shaped with a strength of 25 G/cm at their midpoint and durations of $G_{1,2,3,4} = 0.3, 0.4, 0.6$, and 0.25 ms. The ¹³C carrier is positioned at 46 ppm, the ¹³CO carrier at 177 ppm, and the ¹⁵N carrier at 116.5 ppm.

between time points c and d, modulates the amplitude of these terms:

$$\mathbf{H}^{\alpha}_{x}\mathbf{C}^{\alpha}_{y} \to \cos(\omega_{\alpha}T_{2})\mathbf{H}^{\alpha}_{x}\mathbf{C}^{\alpha}_{y}$$
(1a)

$$\mathbf{H}^{\alpha}_{y}\mathbf{C}^{\alpha}_{y}\mathbf{H}^{\beta}_{z} \rightarrow \cos(\omega_{\beta}t_{2})\mathbf{H}^{\alpha}_{y}\mathbf{C}^{\alpha}_{y}\mathbf{H}^{\beta}_{z}$$
(1b)

where ω_{α} and ω_{β} are the angular offset frequencies of the H^{α} and H^{β} spins. As discussed below, the effect of homonuclear J-dephasing during the short t_2 evolution periods (ca. 12 ms, in practice) is very small and has therefore been ignored in eq 1. During the subsequent delay, $2\delta'$, a $\cos(2\pi J_{\alpha\beta}\delta')$ fraction of the product in eq 1a is converted back to in-phase H^{α}_{ν} magnetization at time point f and, similarly, a $-\sin(2\pi J_{\alpha\beta}\delta')$ fraction of eq 1b is converted back to in-phase H^{α}_{ν} . Thus, at time f there are two contributions to the in-phase H^{α}_{ν} magnetization: a $\cos(2\pi J_{\alpha\beta}\delta) \cos(2\pi J_{\alpha\beta}\delta')$ fraction is modulated in amplitude by $\cos(\omega_{H\alpha}t_2)$ and gives rise to a diagonal resonance, and a $-\sin(2\pi J_{\alpha\beta}\delta)$ $\sin(2\pi J_{\alpha\beta}\delta')$ fraction is modulated by $\cos(\omega_{H\beta}t_2)$, yielding the $H^{\alpha}-H^{\beta}$ cross peak. In order to eliminate other terms, which have been ignored in the above discussion, this magnetization is subjected to a z filter¹³ prior to detection (between times f and g). The relative amplitude of the cross peak $(I_{\rm C})$ versus diagonal peak $(I_{\rm D})$ is

$$I_{\rm C}/I_{\rm D} = -\tan(2\pi J_{\alpha\beta}\delta) \tan(2\pi J_{\alpha\beta}\delta') \approx -\tan^2[\pi J_{\alpha\beta}(\delta+\delta')]$$
(2)

Between time points b and c and between d and e, ${}^{13}C^{\alpha}$ spin operators are part of ${}^{1}H^{\alpha} - {}^{13}C^{\alpha}$ multiple-quantum coherence and ${}^{1}J_{H\alpha C\alpha}$ therefore has no effect on the evolution of the spin system. Also, as was the case for the ¹⁵N spin in the HNHA experiment,⁹ it is easily seen that long-range J coupling between ${}^{13}\bar{C}^{\alpha}$ and H^{β} does not give rise to observable magnetization and merely results in a small attenuation of both diagonal and cross peaks. Similarly, in the case where there are two nonequivalent methylene protons, $H^{\beta 2}$ and $H^{\beta 3}$, J coupling between H^{α} and $H^{\beta 3}$ attenuates both the diagonal resonance and the $H^{\alpha}/H^{\beta 2}$ cross peak by the same factor, $\cos(2\pi J_{\alpha\beta3}\delta)$ $\cos(2\pi J_{\alpha\beta3}\delta')$, leaving eq 2 unchanged. Analogously, if the amide proton has not been exchanged with D_2O , both the diagonal and H^{α}/H^{β} cross peaks are attenuated by $\cos(2\pi J_{\text{H}\alpha\text{H}N}\delta)\cos(2\pi J_{\text{H}\alpha\text{H}N}\delta')$, again leaving the diagonal to cross peak intensity ratio unchanged. In this latter case, there will also be a H^N-H^α cross peak with an $I_C/$ $I_{\rm D}$ ratio given again by eq 2, but substituting $J_{\rm H\alpha HN}$ for $J_{\alpha\beta}$. Note, however, that the HACAHB-COSY experiment is performed preferably in D₂O solution because suppression of the H_2O solvent resonance is non-trivial.

Evolution of the ${}^{13}C^{\alpha}$ chemical shift between time points b and e gives rise to a modulation of the observed signal by $\cos[\omega_{C\alpha}(2t_1^a + 2t_1^b)]$ which is used to disperse the H^{α}-H^{β} correlations into a third frequency dimension. The optimal choice of T^{I} and T^{II} is dictated by the requirement that $2(T^{I} +$ T^{II} = n/J_{CC} with (n = 1, 2, ...), where J_{CC} is the one-bond ${}^{13}C^{\alpha} - {}^{13}C^{\beta} J$ coupling (~35 Hz). For programming convenience it is also desirable that $\delta' < T^{II} < \delta$ and $\delta - \Delta < T^{I} < \delta' - \Delta'$. The t_1 evolution period is of the constant-time type,¹⁴ and J_{CC} evolution causes no t_1 modulation. However, this coupling is active during t_2 , resulting in a J_{CC} doublet splitting in the indirectly detected ¹H dimension. As the maximum t_2 duration is typically chosen shorter than $1/(2J_{CC})$, this splitting remains unresolved and merely limits the resolution obtainable in F_2 . H^{α}/H^{β} cross peaks to nonequivalent H^{β} resonances that differ by less than ca. 0.1 ppm are therefore generally not resolved and the corresponding J values cannot be measured individually.

Pulsed Field Gradients. The intrinsic sensitivity of the HACAHB-COSY experiment is quite good, and the resolution in the ${}^{13}C^{\alpha}$ dimension is also very high, provided that the entire duration of the constant-time t_1 evolution period (~28 ms) is utilized. This latter condition requires the use of a large number of increments in the t_1 dimension and, to keep the measurement time within reasonable limits, it is necessary to restrict the phase cycling to at most eight steps. Therefore, pulsed field gradients are used in the standard manner^{15,16} to minimize artifacts associated with pulse imperfections. Specifically, the first 180° ¹H pulse is sandwiched between two pairs of gradient pulses, G_1 and G_2 , so that at time c only magnetization that has been refocused by this 180° pulse is present. Similarly, the last 180° ¹H pulse is preceded and followed by gradients G_3 and G_1 , so that at time f all ¹H terms of interest are refocused. As G_3 and G_1 are of opposite phase, their sum is smaller than the largest of these two gradients (G_3) but still sufficient to dephase any ¹H terms that have not experienced the last 180° ¹H pulse. On the ¹³C channel, the first 180° pulse is surrounded by gradients G₂, the 180° $_{\phi_3}$ pulse by gradients G₁, and the last 180° pulse by gradients G₃. Finally, gradient G₄, applied during the z filter delay, eliminates any non-longitudinal terms, except for possible small amounts of homonuclear zero-quantum coherence.

Effects of Relaxation and Passive J Coupling. Equation 2 applies to the ratio of the integrated peak intensities. The line shapes in the $F_1({}^{13}C^{\alpha})$ and $F_3({}^{1}H^{\alpha})$ dimensions are identical for cross peaks and diagonal peaks, however. As shown below, the line shape in the F_2 dimension is primarily determined by the short duration of the t_2 acquisition time needed to avoid introduction of a ${}^{1}J_{C\alpha C\beta}$ splitting in this dimension. The signal in the t_2 dimension decays as a result of transverse relaxation and dephasing caused by ${}^{1}J_{C\alpha C\beta}$ and ${}^{1}H^{-1}H$ J couplings. Although this decay does not change the integrated intensity, it attenuates the height of the H^{β} cross peak relative to the H^{α}

⁽¹³⁾ Sørensen, O. W.; Rance, M.; Ernst, R. R. J. Magn. Reson. 1984, 56, 527-534.

⁽¹⁴⁾ Santoro, J.; King, G. C. J. Magn. Reson. 1992, 97, 202-207.
(15) Bax, A.; Pochapsky, S. S. J. Magn. Reson. 1992, 99, 638-643.

⁽¹⁶⁾ Wider, G.; Wüthrich, K. J. Magn. Reson. Ser. B 1993, 102, 239-241

diagonal peak by a factor C, given by

$$C = \int_{t_2=11}^{AT_2} \Pi_k \cos(\pi J_{j\beta k} t_2) \cos(\pi J_{CC} t_2) F(t_2)$$

$$\exp(-t_2/T_{2j\beta}) dt_2 / \int_{t_2=11}^{AT_2} \Pi_j \cos(\pi J_{\alpha j} t_2) \cos(\pi J_{CC} t_2) F(t_2)$$

$$\exp(-t_2/T_{2\alpha,MQ}) dt_2 \quad (3)$$

where the first product extends over all protons, k_i that are coupled to H^{4} , including H^{α} and H^{γ} protons and a possible geminal $\mathbf{H}^{\mathbf{i}}$ spin. The second product extends over all protons, *l*, coupled to H^{α} . AT t is the acquisition time in the t dimension, $J_{\rm CC}$ is the one-bond ${}^{13}{\rm C}^{\alpha}$ – ${}^{13}{\rm C}^{\beta}$ J coupling, $T_{2\beta}$ and $T_{2\alpha,{\rm MO}}$ are the transverse relaxation times of H^{β} and $H^{\alpha} = C^{\alpha}$ two-spin coherence, and $F(t_2)$ is the digital filter applied to the t_2 time domain. Using AT₂ = 12 ms, a cosine bell $F(t_2)$ filter, $T_{2\beta}$ = 30 ms, and $T_{2\alpha,MO} = 100$ ms, one finds from expression 3 that even in the unfavorable case of a value residue, with six H^{γ} protons $(J_{\mu\gamma} = 7 \text{ Hz})$ and a $J_{\alpha\beta}$ value of 10 Hz, the value of C (0.89) is only little affected by the passive spin couplings and transverse relaxation. For a shorter $T_{2\beta}$ value of 15 ms and $T_{2\alpha,MQ} = 50$ ms, C reduces to 0.83. In practice C is dominated by the effect of $T_{2\beta}$; in the absence of T_2 relaxation one finds C = 0.97 for this value spin system. The above example illustrates that the cross peak to diagonal peak height ratio in practice will be attenuated by 3-17% relative to the ratio of the integrated intensities, resulting in underestimates of $J_{\alpha \beta}$ by 2-8%. As, in our experience, the peak heights can be measured more reliably than their integrated intensities, particularly in the case of partial overlap, we prefer deriving $J_{\alpha\beta}$ from the ratio of the peak heights, rather than from the integrated intensities. As argued above, the error introduced by the difference in F_2 line width of the diagonal and cross peaks is small and can be accounted for easily.

A more serious source of error in quantitating $J_{\alpha\mu}$ couplings from the HACAHB-COSY spectrum stems from the faster relaxation of antiphase magnetization relative to in-phase coherence during the de- and rephasing periods, 2δ and $2\delta'$: The diagonal peaks result from terms, $H^{\alpha}{}_{3}C^{\alpha}{}_{y}$, that are in-phase relative to H^{β} during the 2 δ and 2 δ' periods (eq. 1a). H^{α}-H^{β} cross peaks result from terms that become antiphase with respect to H^{μ} ($H^{\alpha}_{\nu}C^{\alpha}_{\nu}H^{\beta}_{-}$) during the period 2δ and that return to inphase during $2\delta'$ (eq 1b). Due to relatively rapid ${}^{1}H - {}^{1}H$ spin flips in proteins, the faster relaxation of $H^{\alpha}{}_{\nu}C^{\alpha}{}_{\nu}H^{\mu}{}_{\tau}$ compared to $H^{\alpha}_{\nu}C^{\alpha}_{\nu}$ can result in a significant attenuation of the cross peak relative to the diagonal peak. This effect has previously been described in detail for the HNHA experiment," and for quantitating the J coupling between Leu 10 C⁹ and 3 H^{β}.¹⁷ It increases approximately linearly with the rotational correlation time of the protein and results in an underestimate of the Jcoupling. This is a general phenomenon that applies to nearly all types of J coupling measurements in macromolecules.¹⁸ For the case of two nonequivalent methylene protons, H^{μ_2} and H^{β_3} . rapid $H^{\beta 2} = H^{\beta 0}$ spin flips can actually convert $H^{\alpha}_{\ \nu} C^{\alpha}_{\ \nu} H^{\beta 2}_{\ z}$ antiphase terms into $H^{\alpha}_{\nu}C^{\alpha}_{\nu}H^{\mu}_{\nu}$, thereby decreasing the intensity of the largest cross peak but increasing the intensity of the weaker of the two H^{α} -H^{β} cross peaks.¹⁷ Numerical calculations based on equations in refs 9 and 17 indicate that for a protein with a rotational correlation time of 7 ns and a generalized order parameter, S^2 , of 0.8, a *trans* $J_{\alpha\beta2}$ coupling to a H^{$\beta2$} methylene proton is underestimated by $\sim 15-20\%$. The magnitude of the measured value for the smaller gauche coupling, $J_{\alpha\beta\beta}$, is less affected in such cases as the increase of $H^{\alpha}{}_{\nu}C^{\alpha}{}_{\nu}H^{\beta}{}_{\tau}$ caused by



Figure 2. Comparison of a small region of the 600 MHz 2D in-phase HACAHB-COSY spectrum of TGF- β 1, recorded (A) with the scheme of Figure 1, without incrementing t_1 , and (B) with a single-quantum analog of this experiment (see Experimental Section). Diagonal and cross peaks have opposite signs.⁹⁻¹¹

 $H^{\beta 2}-H^{\beta 3}$ spin flips is partially offset by a decrease caused by spin flips between $H^{\beta 3}$ and protons other than H^{α} and $H^{\beta 2}$.

Results and Discussion

The improvement in the relaxation behavior of ${}^{1}H^{-1}C$ multiple-quantum coherence over single-quantum coherence is demonstrated for a sample of the homodimeric protein TGF- β 1 (25 kDa). The protein has been derived from mammalian cells and only about half of its residues are enriched in ¹¹C. Figure 2A shows a small region of the in-phase 2D $^{1}H^{-1}H$ COSY spectrum, recorded with the scheme of Figure 1. Strips taken from the corresponding 3D spectrum are given as supplementary material. As the spectrum shown in Figure 2 is not dispersed in the ${}^{10}C$ dimension, most of the diagonal H^{α} resonances overlap but numerous intense cross peaks to previously assigned¹⁹ H^{β} resonances are well resolved. In contrast, if the experiment is carried out without generating heteronuclear multiple-quantum coherence (Figure 2B), diagonal resonances are approximately 4-fold weaker and, except for V98 and V89, cross peaks fall below the noise threshold. The slower relaxation rate applies to the period $2(T^{\dagger} + T^{\dagger})$, which equals 28 ms, indicating a heteronuclear ${}^{1}\mathrm{H}^{\alpha}-{}^{13}\mathrm{C}^{\alpha}$ dipolar contribution to the Hⁿ transverse relaxation rate of $\ln(4)/0.028 \approx 50 \text{ s}^{-1}$, corresponding to a rotational correlation time of ~ 12 ns. This correlation time falls in the range expected for a 25 kDa protein and the decrease in relaxation therefore agrees with theoretical predictions.

The use of the 3D HACAHB-COSY scheme for measurement of $J_{\alpha\beta}$ is illustrated for a sample of uniformly ¹³C-enriched Ca²⁺free calmodulin (148 residues) at 23 °C. This protein presents a more challenging test for the practical use of the method than TGF- β 1, because it has been enriched uniformly in ¹³C, and in the absence of Ca²⁺ the ¹H^{α}-¹³C^{α} correlation spectrum of this highly α -helical protein is very poorly dispersed. Figure 3 shows F_2 strips taken from the 3D spectrum at the ¹³C^{α} (F_1) and ¹H^{α} (F_3) frequencies of residues Q41–I52. For Q41, for example, the H^{α}-H^{β 2} cross peak intensity corresponds to $J_{\alpha\beta2}$ = 9.3 Hz. The absence of an H^{α}-H^{β 3} cross peak, even at lower contour levels, indicates that $J_{\alpha\beta3}$ < 3.5 Hz, diagnostic of a *gauche* coupling.

⁽¹⁷⁾ Vuister, G. W.; Yamazaki, T.; Torchia, D. A.; Bax, A. J. Biomol. NMR 1993, 3, 297-306.

⁽¹⁸⁾ Harbison, G. J. Ann. Chem. Sur. 1993, 115, 3026-3027.

⁽¹⁹⁾ Archer, S. J.; Bax, A.; Roberts, A. B.; Spom, M. B.; Ogawa, Y.; Piez, K. A.; Weatherbee, J. A.; Tsang, M. L.-S.; Lucas, R.; Zheng, B.-L.; Wenker, J.; Torchia, D. A. *Biochemistry* **1993**, *32*, 1152–1163.



Figure 3. F_2 strips from the 600 MHz 3D HACAHB-COSY spectrum of 1.7 mM Ca²⁴-free calibodulin in D₂O. The center of each square box indicates the position of a H³ resonance. Overlapping hoxes are partially dashed. Thus, even though the H^{*t*} protons of Pro⁴³ are not resolved, it is clear that the *J* coupling is larger to H^{*t*3} than to H^{*t*2}. The diagonal and cross peaks of Glu⁴⁷ partially overlap with those of Glu⁸⁷ and Glu³⁷⁰. A total of 114 $J_{\alpha\mu}$ couplings could be measured quantitatively, and for 37 cases the absence of a cross peak indicated $J_{\alpha\mu} <$ ~4 Hz.

 $J_{\alpha \mu}$ values measured from the 3D spectrum for 10 of the alanines in the ordered region of calmodulin all fall in the 5.6-6.2 Hz range, substantially below the 7 Hz value expected for this coupling. In contrast, the intensity ratio for the highly mobile N-terminal alanine indicates a value of 6.9 Hz. The same experiment applied to human ubiquitin, which has a relatively fast rotational correlation time of ca. 4.5 ns, yielded $J_{\alpha\beta}$ values of 6.5 Hz for its two alanines. As discussed above, this reduction in the measured J coupling relative to its true value is caused by the faster relaxation of antiphase terms, compared to in-phase magnetization, which results in a decrease of the cross peak to diagonal peak intensity ratio. Except for highly mobile residues, which are easily recognized because of their very intense diagonal intensity, the underestimate of the $J_{\alpha i}$ coupling caused by this relaxation effect is relatively uniform throughout the protein. Nearly all methods for measurement of small J couplings in proteins are affected by the faster relaxation of antiphase versus in-phase magnetization.¹⁸ Comparison of the J_{tyl} values measured in human ubiquitin using the HACAHB-COSY scheme with the values obtained from a ¹³C^α separated E. COSY scheme²⁰ indicates that the HACAHB-COSY data are less affected by this relaxation effect than the corresponding E. COSY spectra (A. C. Wang, unpublished results).

In combination with heteronuclear ${}^{15}N-{}^{1}H^{\beta}$ and ${}^{13}C'-{}^{1}H^{\beta}$ three-bond J couplings and/or NOE cross peak intensities, $J_{\alpha\beta}$ values can be used for making stereospecific assignments of the H^{β} methylene protons and for determining the rotameric states around the C^{α}-C^{β} bonds in proteins. Although other methods for measuring this coupling have been described in recent years, ${}^{20-22}$ for larger proteins the present method in our experience compares favorably in sensitivity and in spectral simplicity. The data presented in Figure 2 convincingly demonstrate the gain in sensitivity that can be obtained by using the slower relaxation rate of ${}^{3}H-{}^{13}C$ multiple-quantum coherence compared to that of the ${}^{1}H$ single-quantum coherence. The same idea can be incorporated in numerous other multidimensional heteronuclear NMR experiments and may further increase the size limit of proteins that can be studied in detail by multi-dimensional heteronuclear NMR.

Experimental Section

The sample of TGF- β 1 was obtained from overexpression in Chinese harnster ovary cells, grown on a medium containing uniformly ¹⁵N/ ¹³C-corriched Leu, Ile, Val, Pro, Tyr, Phe, Scr. and Gly residues. The levels of ¹³C enrichment for these residues in the purified protein caried hetween 65 and 90%. Details regarding the sample preparation have heen given previously.¹⁹ The sample used for recording the spectra of Figure 2 contained 4 mg of TGF- β 1 in D₂O (0.8 mM dimer), p²H 4.2, in a 200 µL Shigemi microcell (Shigemi Inc., Allison Park, Pa).

The sample of uniformly ${}^{13}C/{}^{15}N$ -enriched *Xenopus* calmodulin was obtained from overexpression in *Excherichia coli*, grown on a medium containing ${}^{13}C_6$ -glucose and ${}^{13}NH_4Cl$. The NMR sample contained 11 mg of protein in 390 μ L of D₂O (1.7 mM), 150 mM KCl, and 1.5 mM EDTA, p²H 6.3.

NMR spectra were recorded on a Bruker AMX-600 spectrometer, equipped with a triple-resonance prohehead that contained a self-shielded z-gradient coil. TGF- β 1 spectra were recorded at 45 °C and calmodulin spectra at 23 °C.

The 2D TGF- β 1 spectra shown in Figure 2 each result from a 54* × 384* data matrix, with acquisition times of 12 nts (t₂) and 53 ms (t₃), keeping $t_1 = 0$. Measuring time: 4 h per spectrup). The data were apodized in the H^{a/ff} dimension with a 65°-shifted sine hell window and zero-filled to 256*. In the detected dimension, data were apodized by a 65°-shifted squared sine hell window and zero filled to 1024*. The spectrum of Figure 2A was recorded with the scheme of Figure 1, keeping t_1 constant. The spectrum of Figure 2B was recorded with a single-quantum analog of the HACAHB-COSY scheme, where the ¹³C pulses of Figure 1 were not applied (except for ¹³C decoupling during data acquisition), and the two 90° ¹H pulses flanking the t_2 evolution period were incremented hy 90° relative to the scheme of Figure 1. In addition, a 90°_x=90°_{φ3} pair of ¹³C pulses ($\phi_3 = x, -x$), inserted $1/(2^3 J_{CO})$ after the first ¹H 90_{φ1} pulse, serves as a ¹³C filter²³ (receiver = x, 2(-x).

The 3D HACAHB-COSY spectrum of calmodulin results from a $50^* \times 54^* \times 384^*$ data matrix with acquisition times of 23.2 ms (t_1) , 12 ms (t_2) , and 53 ms (t_3) . The total number of scans for each hypercomplex t_3/t_2 increment was 32, and the total measuring time was 24 h. The data processing in the t_2 and t_3 dimensions was the same as described above for TGF- β 1. In the t_3 dimension, the number of t_1 data points was doubled by mirror intage linear prediction.²⁴ prior to cosine-squared bell apodization. The digital resolution of the linal 3D spectrum was 8.4 Hz (F_1) , 17.7 Hz (F_2) , and 7.2 Hz (F_3) .

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Supplementary Material Available: The listing of the Bruker AMX pulse program for the HACAHB-COSY experiment and a figure showing strips taken from the 3D HACAHB-COSY spectrum of TGF- β 1 for the residues with cross peaks in the region shown in Figure 2 of the manuscript (4 pages). This material is contained in many libraries on microfiche, immediately follows this article in the microfilm version of the journal, can be ordered from the ACS, and can be downloaded from the Internet; see any current masthead page for ordering information and Internet access instructions.

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¹²⁰⁾ Eggenberger, U.: Kariad-Nejad, Y.: Thäriag, H.: Röterjans, H.: Griesinger, C. J. Biomol. NMR **1992**, 2, 583-590.

⁽²¹⁾ Gemmecker, G.; Fesik, S. W. J. Magon. Reson. 1991, 95, 208-213.
(22) Emerson, S. D.; Montelione, G. T. J. Am. Chem. Soc. 1992, 114, 354-356.

⁽²³⁾ Oning, G.; Wührich, K. Q. Rev. Biophys. 1990, 23, 39-96,
(24) Zhu, G.; Bax, A. J. Magn. Reson. 1990, 90, 405-410.
(25) McCoy, M.; Mueller, L. J. Am. Chens. Soc. 1992, 114, 2108-2112.